

ORIGINAL ARTICLES

Design and development of diltiazem hydrochloride transmucosal drug delivery system

Návrh a vývoj systému pro transmukózní přívod diltiazem hydrochloridu

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Summary

Diltiazem hydrochloride is an antihypertensive agent which undergoes extensive first pass metabolism making it a possible candidate for buccal delivery. Diltiazem mucoadhesive buccal patches were prepared using HPMC, chitosan, PVP, PVA and carbopol. The physicochemical interactions between diltiazem and the polymers were investigated by FTIR and DSC, results revealed no interaction between drug and polymers. The patches were evaluated for various physicochemical parameters, *in vitro* release studies and *ex vivo* permeation through porcine buccal mucosa. Residual solvent content in patches was determined by gas chromatography and are largely below the tolerated limits. The formulations showed an extended release of the drug upto a period of 12 hours during *ex vivo* permeation and showed non Fickian drug release. Stability of the optimized formulation was investigated as per ICH guidelines and was found to be stable with respect to drug content and *ex vivo* permeation.

Keywords: diltiazem hydrochloride • buccal patches • residual solvents • mucoadhesion • *in vitro* drug release • *ex vivo* permeation

Souhrn

Diltiazem hydrochlorid je antihypertenční látka, která vykazuje značný first pass metabolismus, a to ji činí vhodným kandidátem pro bukální podání. Mukoadhezivní bukální náplasti byly připraveny s HPMC, chitosanem, PVP,

PVA a carbopolem. Fyzikálně-chemické interakce mezi léčivem a polymery byly sledovány pomocí FTIR a DSC: stanovení neprokázala žádné interakce mezi diltiazem hydrochloridem a polymery. U bukálních náplastí se stanovily různé fyzikálně-chemické parametry, uvolňování léčiva *in vitro* a permeace *ex vivo* přes bukální sliznici prasete. Zbytkové obsahy rozpouštědel v náplastech se určily plynovou chromatografií a byly pod tolerovanými limity. Při *ex vivo* studii se léčivo z náplastí uvolňovalo rovnoměrně po dobu 12 hodin kinetickým modelem podle Korsmeyer-Peppase. Stabilita optimalizované formulace se zkoumala podle pokynů ICH a z hlediska obsahu léčiva a jeho permeace *ex vivo* vykazovala výborné výsledky.

Klíčová slova: diltiazem hydrochlorid • bukální náplasti • bytková rozpouštědla • mukoadheze, uvolňování léčiva *in vitro* • permeace *ex vivo*

Introduction

Amongst the various routes of drug delivery, the oral route is most preferred to the patient. However, oral administration of drugs has disadvantages such as hepatic first pass metabolism and enzymatic degradation within the GI tract, that prohibit oral administration of certain classes of drugs, especially peptides and proteins. Consequently, other absorptive mucosae are considered as potential sites for drug administration. Transmucosal routes of drug delivery (mucosal linings of nasal, rectal, vaginal, ocular and oral cavity) offers distinct advantages over oral administration for systemic drug delivery. These advantages include possible bypass of first pass effect, avoidances of pre-systemic elimination within the GI tract and better enzymatic flora for drug absorption^{1–3}). Though the rectal, vaginal and ocular mucosa offer certain advantages, the poor patient acceptability associated with these sites renders them reserved for local applications rather than systemic drug administration. The oral cavity, on the other hand, is highly acceptable by the patient, the mucosa is relatively permeable with rich blood supply, it is robust and shows a short recovery time after stress or damage^{4–6}) and the virtual lack of Langerhans cells make

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Table 1. Composition of diltiazem hydrochloride buccal patches

Ingredients	Formulation			
	F1	F2	F3	F4
Diltiazem (mg)	500	500	500	500
Chitosan (mg)	150	150	150	150
HPMC K15M (mg)	225	–	–	–
PVP (mg)	–	225	–	–
PVA (mg)	–	–	225	–
Carbopol 934P (mg)	–	–	–	225
Dimethylsulphoxide (ml)	0.2	0.2	0.2	0.2
Propylene glycol (ml)	0.4	0.4	0.4	0.4
1% Acetic acid (ml)	5	7.5	7.5	7.5
Methanol (ml)	5	–	–	–
Dichloromethane (ml)	5	–	–	–
Ethanol (ml)	–	–	–	7.5
Water (ml)	–	7.5	7.5	–

the oral mucosa tolerant to potential allergens. Furthermore, oral transmucosal drug delivery bypasses first pass effect and avoids presystemic elimination in the GI tract. These factors make the oral mucosal cavity a very attractive and feasible site for systemic drug delivery.

Diltiazem is an effective calcium channel blocker, used in the treatment of angina, hypertension and myocardial infarction. It was reported to be rapidly absorbed after oral administration, but it undergoes extensive first pass metabolism leading to poor bioavailability (40%). In addition, diltiazem hydrochloride has a low dose (30 mg), low molecular weight (451) and an extensive first pass effect; a need for long term treatment and repetitive dosing⁷). All these parameters make this drug an interesting candidate for buccal administration.

Experimental part

Material and methods

Diltiazem hydrochloride (BP) was a gift from Nicholas Piramil (Kohir, India). Chitosan (food grade, deacetylation value: more than 85% and molecular weight: 15000) was a generous gift from Marine Chemicals (Cochin, India); Hypromellose (HPMC K15M: Molecular weight: 10.000–1.500.000; Viscosity: 15.000 cP) and Carbomer (carbopol 934P; Viscosity: 29,400–39,400 cP) was obtained from Tini Pharma Ltd., (Tirupathi, India); Polyvinyl alcohol (Molecular weight: 20000, Viscosity: 4–7 cP) was obtained from Loba Chemie Pvt. (Mumbai, India) and Povidone (Polyvinyl pyrrolidone K30; Molecular weight: 50000, Viscosity: 5.5–8.5 cP) was gifted by the International Specialty Products (Hyderabad, India). All reagents and solvents used were of analytical grade.

Investigation of drug-excipient interactions

Fourier transform infrared spectroscopy

Compatibility between the drug and the polymers was studied by FTIR spectra. FTIR studies were carried out

for drug and its physical mixture (1 : 1). The sample was dispersed in KBr powder and the compacts were made by applying 6000 kg/cm² pressure and analyzed. FTIR spectra were obtained by diffuse reflectance on a FTIR spectrophotometer type FTIR 8400 (Schimadzu Corporation, Japan). The positions of FTIR bands of important functional groups of drug were identified and were cross-checked in obtained spectra.

Differential scanning calorimetry (DSC)

DSC studies for the drug and its physical mixture (1 : 1) were carried out using a DSC-60 calorimeter (Schimadzu Corporation, Japan). The instrument was calibrated with an indium and zinc standard. The sample was heated from 10 to 300 °C at a heating rate of 25 °C/min to remove thermal history. The sample was then immediately cooled to 10 °C and reheated from 10 to 300 °C under the flow of nitrogen at a heating rate of 10 °C/min.

Preparation of patches

Diltiazem hydrochloride mucoadhesive buccal patches were prepared by solvent casting technique using chitosan, hydroxypropyl methyl cellulose (HPMC K15M), polyvinyl pyrrolidone (PVP K30), polyvinyl alcohol (PVA) and carbopol 934P as polymers. Propylene glycol and dimethyl sulfoxide (DMSO) were used as the plasticizer and penetration enhancer, respectively. Acetic acid, ethanol, methanol and dichloromethane (DCM) were used as solvents. The composition of samples used for the preparation of buccal patches is shown in Table 1. The drug was dissolved in a small quantity of solvent and polymers were dissolved in the remaining solvent/solvent mixture. The drug, polymer solutions along with the plasticizer and permeation enhancer were sonicated for 30 min and examined for air entrapment. The solution was poured onto glass moulds of 10 x 5 cm² and air-dried for overnight at room temperature. An inverted funnel was kept on the mould for controlled evaporation. The dried film of the drug was peeled from the mould and packed

in an aluminium foil and kept in a desiccator till further use.

The backing layer was also prepared by the solvent casting method by dissolving 500 mg ethylcellulose in 15 ml of an ethanol-toluene mixture (1 : 4). The medicated patches were laminated on one side with the backing layer and used for release studies.

Drug content

Drug content of patches was determined by dissolving five patches (1 cm²) in 100 ml of phosphate buffer of pH 6.6. After suitable dilutions the resultant solution was filtered and analysed for diltiazem content spectrophotometrically using a UV-1700 Pharma Spec spectrophotometer, Shimadzu Corporation, Japan at 237 nm.

Thickness and weight variation^{8,9)}

The thickness of patches was assessed using a micrometer screw gauge (Mitutoyo, Japan). From each formulation, three randomly selected patches with a surface area of 1 cm² were used. Each patch was weighed individually on an analytical balance (Shimadzu, Japan) and the average weights were calculated.

Folding endurance¹⁰⁾

Folding endurance of patches was determined manually by repeatedly folding a film at the same place until it breaks. The number of foldings required to break or crack a patch was taken as the folding endurance.

Surface pH¹¹⁾

Patches were placed in Petri dishes containing 5 ml phosphate buffer (pH 6.6) and the pH at the surface was measured by placing the tip of the glass microelectrode of a digital pH meter (Elico LI 120, India) close to the surface of the patch and allowing it to equilibrate for 1 min prior to recording. Experiments were performed in triplicate.

Swelling index¹²⁾

Swelling index of the patches was evaluated by placing them in Petri dishes containing 4 ml of phosphate buffer pH 6.6 at room temperature. The patches were taken at regular intervals from the Petri dish and excess buffer was removed using filter paper. The swollen system was reweighed (w_2). The difference between the initial weight (w_1) and the weight gained at regular time interval (w_2) was used to determine the swelling index which was calculated as $S.I. = (w_2 - w_1/w_1) \times 100$.

Preparation of porcine buccal mucosa¹³⁾

Buccal tissue was obtained from a local slaughterhouse from a freshly sacrificed porcine and used within 3 to 4 hr of sacrifice. The tissue was stored in isotonic phosphate buffer (pH 7.4) at 4 ± 1 °C upon collection. The epithelium was separated from the underlying connective tissue using a surgical blade and the membrane was used for the experiments.

***In vitro* residence time¹⁴⁾**

In vitro residence time was determined according to the method described by Nafee et al. The apparatus consists of a disintegration apparatus with 800 ml of phosphate buffer pH 6.6 maintained at 37 ± 1 °C. Porcine buccal mucosa was glued to the glass slide and held vertically in the apparatus. The buccoadhesive patch was hydrated with 0.5 ml of phosphate buffer pH 6.6 and the hydrated surface was brought in contact with the buccal mucosa and pressed by applying pressure with the thumb for 5 min. The glass slide was allowed to move up and down (28–32 strokes per minute) so that the patch was completely immersed in the buffer solution at the lowest point and was out at the highest point. The time required for the complete erosion or detachment of the patch from the mucosal surface was recorded.

***In vitro* mucoadhesion test**

In vitro bioadhesion of the patches was determined by the procedure of Varsha et al.¹⁵⁾ using porcine buccal mucosa. A piece of porcine buccal mucosa was cut and glued with a commercially available adhesive on the ground surface of a tissue holder made of thin plastic sheet. Similarly, the patch was glued to another tissue holder of the same size. Then the tissue holders with porcine buccal mucosa and patch were put in contact with each other by applying constant pressure with the thumb for 5 min to facilitate adhesion. The tissue holder with porcine buccal mucosa was allowed to hang on an iron stand with the help of an aluminium wire fastened with the hook provided on the back of the holder. A preweighed lightweight polypropylene bottle was attached to the hook on the back side of the formulation holder with aluminium wire. After a preload time of 5 min, water was added to the polypropylene bottle through an intravenous infusion set at a constant rate. The addition of water was stopped when the buccoadhesive system was detached from buccal mucosa. The weight required to detach the system from buccal mucosa was noted.

The force of adhesion and the bond strength¹⁴⁾ were calculated as:

$$\text{Force of adhesion (N)} = \frac{\text{Weight (g)} \times 9.81}{1000}$$

$$\text{Bond strength (N/m}^2\text{)} = \frac{\text{Force of adhesion (N)}}{\text{Surface area of patch (m}^2\text{)}}$$

Determination of residual solvents

Methanol¹⁶⁾, ethanol¹⁷⁾, dichloromethane¹⁸⁾ and acetic acid¹⁹⁾ content in patches was determined by gas chromatography on an Agilent 7890 Gas Chromatograph, USA, fitted with a flame ionization detector. For estimation of residual solvents, 1 cm² patch was dissolved in a small amount of DMSO in a 10 ml volumetric flask and the volume was made up to 10 ml with DMSO. The solution was filtered through a 0.45 µm filter and degassed using a sonicator. From the sample, 1 µl was

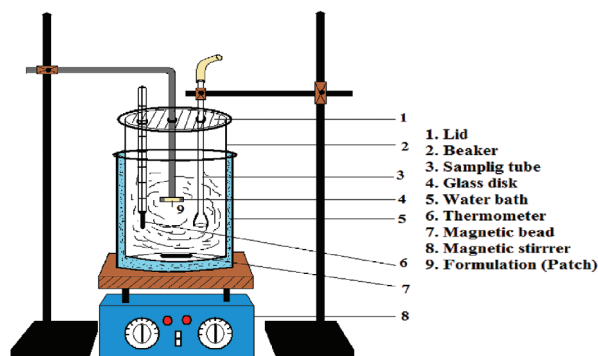


Fig. 1. Modified dissolution apparatus used for *in vitro* release study

injected into the injection port, the chromatogram was recorded and the peak area of the solvent was measured. The concentration of the residual solvent was calculated from calibration curve data.

In vitro release studies¹⁵⁾

The apparatus consists of a receptor compartment (250 ml beaker), which is covered with a thin plastic sheet with three holes, one for a thermometer, second for a sample collection tube and third for a formulation holding pelete glass rod shown in Fig. 1. Before starting the *in vitro* study, the patch was attached to the glass rod and placed four inches above the receptor. The dissolution medium was 100 ml of phosphate buffer pH 6.6. The temperature was maintained at 37 ± 1 °C on a heat-controlled hot plate with a magnetic stirrer. Dissolution fluid was stirred at a constant speed of 50 rpm using a magnetic bead. Samples were withdrawn at regular intervals and the same volume of fresh phosphate buffer pH 6.6 was replaced into the beaker to maintain the constant amount of dissolution medium. The samples were filtered through a 0.45 µm filter paper (Millipore) and drug concentration was analyzed spectrophotometrically. The experiment was carried out in triplicate for each formulation and the mean release was determined.

HPLC analysis²⁰⁾

Analysis of diltiazem was performed using a Shimadzu LC -2010CHT HPLC system equipped with a UV detector and an Inertsil column (150 x 4.6 mm i.d) at ambient temperature. The mobile phase was a mixture of water and acetonitrile (63 : 37) containing 0.35% w/v of triethylamine and the pH was adjusted to 3.0 with 5% orthophosphoric acid. The solution was filtered through a 0.45 µm filter and degassed by sonication. The flow rate was 1 ml per minute. Detection was carried on at 240 nm wavelength. A calibration curve was plotted for diltiazem in the range of 10–50 µg/ml. Good linear relationship was observed between the concentration of diltiazem and its peak area ($r^2 = 0.997$). Precision and accuracy of the HPLC method were estimated.

Ex vivo permeation studies²¹⁾

One cm² patch under study was placed in intimate contact for five minutes with the excised porcine buccal mucosa and mounted between the two compartments of Franz diffusion cell. A teflon bead was placed in the receptor compartment filled with 25 ml of pH 6.6 phosphate buffer. The diffusion cell was thermostated at 37 ± 1 °C and at a rate of 50 rpm. The samples were withdrawn at regular intervals and the same volume of fresh phosphate buffer pH 6.6 was replaced into the diffusion cell to maintain a constant amount of diffusion medium. Samples were filtered through a 0.45 µm filter paper (Millipore) and analyzed for drug content using HPLC and the data were statistically analysed by one way ANOVA followed by turkey post hoc test for multiple comparison using graph pad prism. Differences were considered to be significant at a level of $p < 0.05$.

The permeability coefficients (P) were calculated as follows²²⁾:

$$P = (dQ/dt) / (CA),$$

where: dQ/dt – permeation rate, C – concentration of the donor chamber, A – surface area of diffusion.

Steady state fluxes (J_{ss}) were calculated by dividing the slope of the cumulative amount permeated vs. time curve by the diffusional area.

*Drug release from backing layer*²³⁾

A 1 cm² patch was placed between the two compartments of a Franz diffusion cell at 37 ± 1 °C with the backing layer facing the receptor compartment filled with 25 ml of pH 6.6 phosphate buffer. The samples were withdrawn at regular intervals and the same volume of fresh phosphate buffer pH 6.6 was replaced into the diffusion cell to maintain the constant amount of the diffusion medium. Samples were filtered and analyzed for drug content.

Stability in artificial saliva^{24, 25)}

Stability of the patches was assessed in artificial saliva. Patches were placed in Petri dishes containing 5 ml of artificial saliva (composition: Sodium carboxymethylcellulose 10 g, potassium chloride 0.625 g, magnesium chloride 0.059 g, calcium chloride 0.166 g, di potassium hydrogen phosphate 0.804 g, potassium dihydrogen phosphate 0.326 g, methyl p-hydroxybenzoate 2 g and water up to 1000 ml) and kept in a temperature controlled oven at 37 ± 1 °C for 6 h. The patches were examined for changes in texture and drug content.

*Stability studies*²⁶⁾

Stability studies were conducted according to the ICH Q1A (R2) guidelines. Patches were wrapped in an aluminum foil and were kept in a stability chamber at a temperature of 40 ± 2 °C and $75 \pm 5\%$ RH for 6 months. Samples were withdrawn at the end of 6 months and analyzed for drug content and *ex vivo* permeation through

porcine buccal mucosa. The zero time samples were used as control for the study and the results were statistically analyzed by using t-test and $p < 0.05$ were considered as significant.

Results and discussion

Investigation of drug-excipient interactions

FTIR spectral analysis

Diltiazem hydrochloride pure drug and with excipients (F1–F4, Table 1) were subjected to FTIR spectroscopic analysis. The obtained spectra are shown in Fig. 2. Characteristic peaks of diltiazem were compared with the peaks obtained with the physical mixture. The FTIR spectra of pure diltiazem showed sharp characteristic peaks at 781, 839 (C–H out-of-plane), 1679, 1743 (C = O stretch), 2395 (N–H stretch) and 2922, 2971 cm^{-1} (C–H stretch). All the above characteristic peaks appeared in the spectra of physical mixtures at the same wavenumbers indicating no modification or interaction between the drug and polymers.

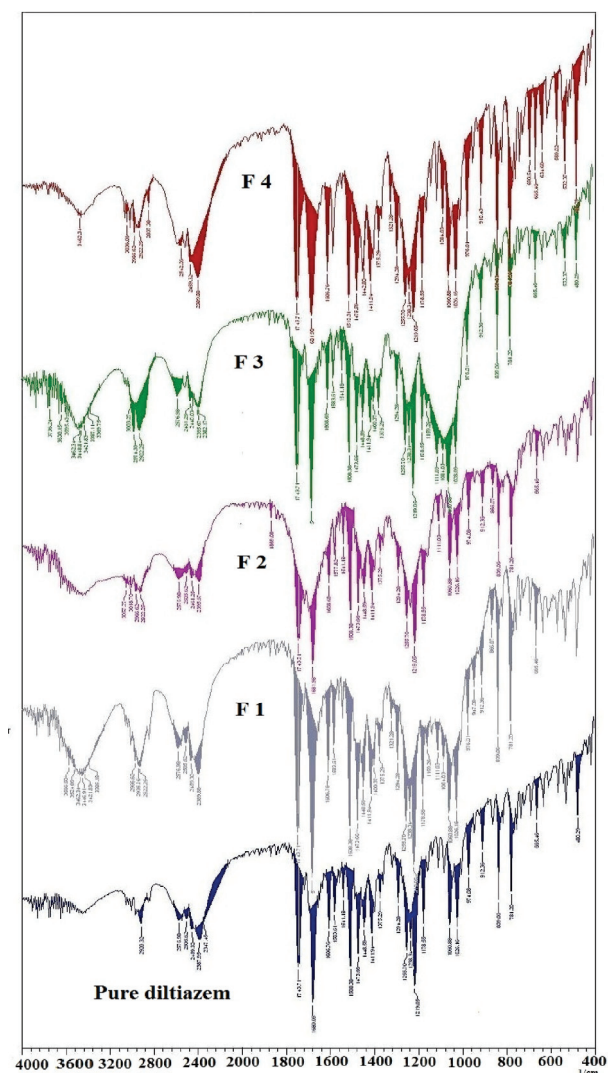


Fig. 2. FTIR spectra of diltiazem and its physical mixture

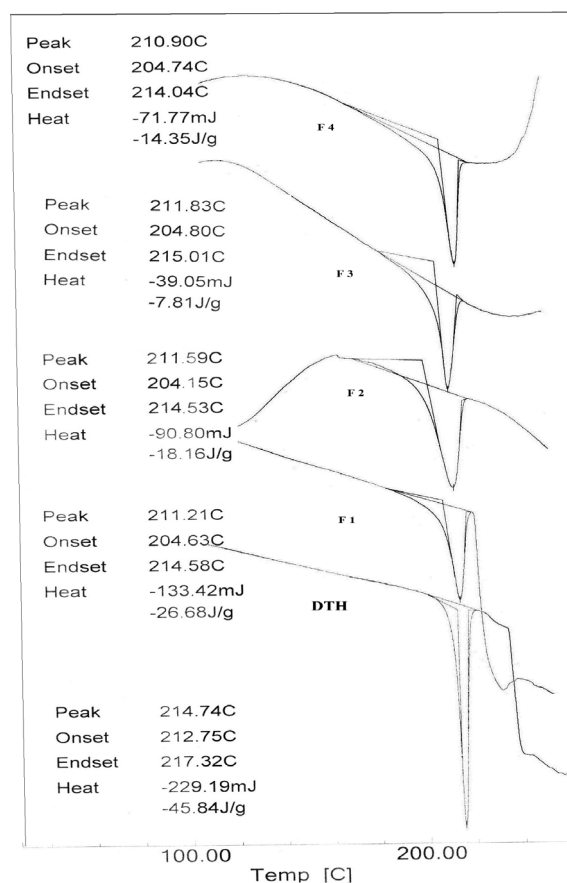


Fig. 3. DSC thermograms of diltiazem and its physical mixture

Differential scanning calorimetry

DSC studies were carried out for diltiazem hydrochloride pure drug and with excipients (F1–F4, Table 1). DSC thermograms obtained are shown in Fig. 3. The DSC thermogram of diltiazem showed an endothermic peak at 214.74 °C corresponding to its melting temperature, which was also detected in the thermograms of the physical mixture, signifying no interaction between diltiazem and the polymers.

Physicochemical evaluation of diltiazem buccal patches

Physicochemical evaluation data are shown in Table 2. The drug content was determined in triplicate and it was found to be uniform in all the patches. The patches (F1 to F4) were weighing in between 27.09 mg to 29.85 mg. Patch thickness was in the range of 257 μm to 323 μm . Folding endurance of the patches was in the following order F1 > F4 > F3 > F2. The folding endurance of all the films was optimal, the films exhibited good physical and mechanical properties. High alkaline or acidic pH of patches may cause irritation to the buccal mucosa and influence the degree of hydration of polymers^{27, 28}), so the surface pH of patches was determined to optimize release and adhesion. The surface pH of all formulations was in the range of 5.9–7 pH, i.e. close to buccal pH. The swelling index of the patches was in the order F1 > F4 > F2 > F3 and showed significant difference. Formulation F1 showed the highest swelling which may be due to the presence of highly swellable

Table 2. Physicochemical evaluation of diltiazem buccal patches

Formulation	Parameter						
	Drug content	Weight variation (mg)	Thickness (μm)	Folding endurance time (min)	Surface pH	Swelling index	<i>In vitro</i> residence
F 1	9.91 \pm 0.205	28.97 \pm 0.51	273 \pm 2.08	286 \pm 4.5 (b***, c***, d**)	6.32 \pm 0.31	54.28 \pm 1.78 (b***, c***, d*)	303 \pm 6.66 (b***, c***, d**)
F 2	10.21 \pm 0.055	27.09 \pm 0.15	293 \pm 2.08	217 \pm 6.5 (a***, d**)	5.94 \pm 0.14 (d*)	32.57 \pm 2.03 (a***, d***)	274 \pm 4.73 (a***, c***, d***)
F 3	10.09 \pm 0.107	28.13 \pm 0.32	257 \pm 3.21	228 \pm 6.55 (a***, d**)	5.99 \pm 0.11 (d*)	29.65 \pm 1.98 (a***, d***)	213 \pm 6.65 (a***, b***, d***)
F 4	9.97 \pm 0.190	29.85 \pm 0.31	323 \pm 2.51	255 \pm 7.5 (a**, b**, c**)	6.66 \pm 0.06 (b*, c*)	46.61 \pm 0.97 (a*, b***, c***)	320 \pm 8.5 (a**, b***, c***)

Mean \pm SD, n = 3. a/b/c/d: Significantly different from F1/F2/F3/F4, respectively, */**/ ***: p < 0.05/p < 0.01/p < 0.001, respectively

HPMC. Formulations F2 and F3 showed faster swelling (with in 45 min) compared to other formulations due to more hydrophilic nature of PVP and PVA²⁹). The high initial uptake of water was observed in F1, F2 and F3 due to a faster hydration rate of polymers. Carbopol will undergo ionization at pH 6.8 and leads to the generation of negative charges at the backbone of the polymer. Repulsion between these like charges leads to uncoiling of the polymer to produce an extended structure capable of greater uptake of water^{23, 30}), which leads to the greater swelling index of F4.

In vitro residence time of the patches was in the order F4 > F1 > F2 > F3 and showed significant difference. A higher residence time in F4 may be due to the presence of carbopol with higher mucoadhesivity than those of other polymers³¹). Whereas the presence of PVP and PVA (hydrophilic polymers) leads to a decrease in the residence time of the patches^{29, 32}). Between F2 and F3, formulation F2 showed a longer residence time which may be due to a greater hydrophilic nature of PVP than that of PVA. And also mucin contains 95% of water³²), so PVP showed more affinity towards mucin. The results are in agreement with earlier reports of Hao et al.³³), Nafee et al.³⁴) and Patel et al.³⁵).

An effective buccal mucosal delivery device must maintain intimate contact with the mucus layer overlying the epithelial tissue. This parameter is critical for successful utilization of these dosage forms. Hence, *in vitro* mucoadhesion testing was performed using the pork mucosal membrane, which gives an indirect measurement of the bioadhesive strength in grams. Table 3 shows the *in vitro* bioadhesive strength of diltiazem patches, the bond

strength values were found to be 951.9, 868.87, 831.56 and 1051.76 N/m² for F1, F2, F3 and F4, respectively, and significant difference was found in bioadhesive strength of patches. F4 showed the greatest bioadhesive strength followed by F1, F2 and F3. Formulations F4 and F1 showed greater bioadhesive strength due to the presence of carbopol and HPMC, respectively³⁶).

According to ICH guidelines, acetic acid and ethanol are class III solvents (solvents with low toxic potential) and the limit of 5000 ppm is acceptable without justification. Methanol, dichloromethane and toluene are class II solvents (solvents to be limited) thus the limits of 3000 ppm, 600 ppm and 890 ppm, respectively, are acceptable. The residual solvents contents in patches are largely below the tolerated limits (Table 4).

In vitro release studies

In vitro release studies of patches were carried out in triplicate. After 6 h the release was found to be 81.84 \pm 2.26, 87.46 \pm 2.9, 86.9 \pm 1.83 and 79.7 \pm 2.36% for the formulations F1, F2, F3 and F4, respectively (Fig. 4). The data of *in vitro* release were analyzed by one way ANOVA and there was no significant difference between means at 30 & 90 minutes. *In vitro* release studies clearly showed that the percent release of diltiazem was maximum, i.e. 87.46% for F2. The order of drug release was found to be F2 > F3 > F1 > F4. All the drug dissolution profiles showed zero order kinetic models with non-Fickian diffusion mechanism.

Ex vivo permeation studies

Ex vivo permeation studies for the patches were carried

Table 3. *In vitro* bioadhesive strength of diltiazem patches

Formulation	Bioadhesive strength		
	Weight (g)	Force of adhesion (N)	Bond strength (N/m ²)
F1	9.703 \pm 0.49	0.0952	951.9
F2	8.857 \pm 0.266 (c*)	0.0869	868.87
F3	8.477 \pm 1.156 (d***)	0.0832	831.56
F4	10.721 \pm 0.66 (b*)	0.1051	1051.76

Mean \pm SD, n = 3. b/c/d: Significantly different from F2/F3/F4 */***: p < 0.05/p < 0.001, respectively

Table 4. Residual solvent content in diltiazem patches

Residual solvent	Limit (ppm)*	Concentration (ppm)			
		F1	F2	F3	F4
Acetic acid	5000	57.792 ± 6.09	55.935 ± 5.66	54.02 ± 5.8	53.702 ± 6.09
Ethanol	5000	–	–	–	63.253 ± 5.64
Methanol	3000	45.378 ± 6.68	–	–	–
Dichloro-methane	600	14.33 ± 4.54	–	–	–

Mean ± SD, n = 3, *As per ICH guidelines

out in triplicate and after 12 hours the release was found to be 76.38 ± 5.11, 84.21 ± 6.42, 80.37 ± 5.03 and 73.71 ± 4.27% for the formulations F1, F2, F3 and F4, respectively (Fig. 5). The data of *ex vivo* permeation were analyzed by one way ANOVA and significant difference was not observed between means up to 360 minutes. In the *ex vivo* permeation study, formulation F2 showed the maximum release of the drug, 84.21% in 720 min; this formulation was considered as the optimized one and used for further study. The order of drug release is F2 > F3 > F1 > F4. F2 showed a greater release followed by F3 which may be due to the presence of hydrophilic polymers PVP and PVA, respectively, which absorb more water and promote dissolution. Moreover, PVP will dissolve and create channels for the drug to diffuse from the patches²⁹). Though F1 showed a greater swelling index, it showed a slow release of diltiazem from the patches, which may be due to high viscous nature of HPMCK15M; a thick gel (diffusion path length) was formed and it acts as a barrier for drug diffusion and slow erosion of the polymer³⁷). F4 also showed a slow release, which may be due to the formation of a thick gel barrier by chitosan and carbopol^{29, 31}).

The drug release data obtained were fitted into the zero order, first order, Higuchi and Korsmeyer-Peppas

equations to know the mechanism of drug release from these formulations. The *ex vivo* permeation profile of F1 and F3 formulations could be best expressed by the Korsmeyer-Peppas model, as the plots showed the highest linearity (r²: 0.9948 and 0.994, respectively), and F2 and F4 formulation could be best expressed by the zero order model, as the plots showed the highest linearity (r²: 0.9968 & 0.9963, respectively). All the formulations showed a non-Fickian release pattern (Table 5) as it was evidenced from the release exponent (n > 0.5), which indicates coupling of the diffusion and erosion mechanism, called anomalous diffusion, and shows that the drug release is controlled by more than one process. So, the suggested drug release mechanism for diltiazem patches may be a combination of diffusion and erosion of the polymer matrix.

The time taken for the permeation of 50% diltiazem was found to be 430, 401, 408 and 466 minutes for the formulations F1, F2, F3 and F4, respectively. The mean steady state flux (J_{ss}) was found to be 0.666 ± 0.05, 0.7149 ± 0.027, 0.6929 ± 0.016, 0.6269 ± 0.04 mg/cm²/hr and the permeability coefficient was found to be 0.0666 ± 0.005, 0.0715 ± 0.003, 0.0693 ± 0.002, 0.0623 ± 0.004 cm/hr (Table 6) for the formulations F1, F2, F3 and F4, respectively.

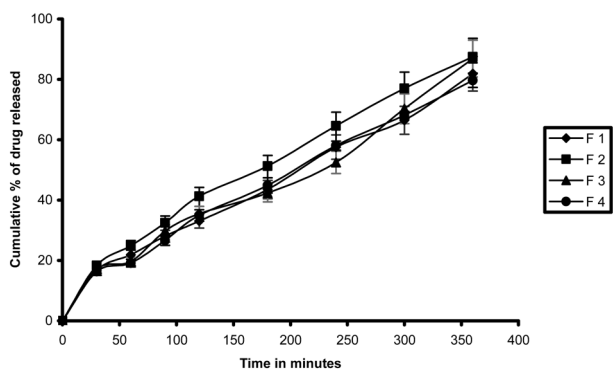


Fig. 4. In vitro drug release profile of diltiazem patches

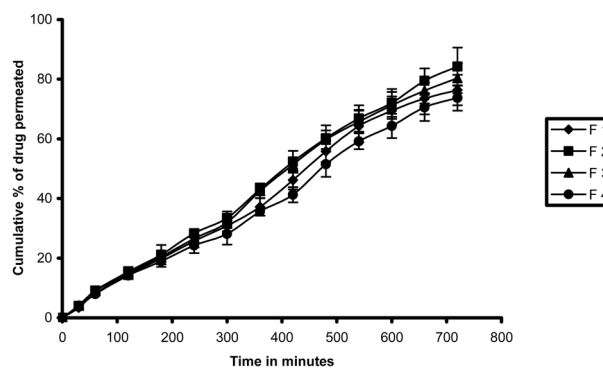


Fig. 5. Ex vivo permeation profile of diltiazem patches

Table 5. Correlation coefficient (r²) and rate constant of different kinetic models for diltiazem patches

Formulation	n value	Correlation coefficient (r ²)				Drug transport mechanism
		Zero order	First order	Higuchi	Peppas	
F1	0.9507	0.9919	0.9649	0.9566	0.9948	Non-Fickian diffusion
F2	0.9412	0.9968	0.9536	0.9641	0.9917	Non-Fickian diffusion
F3	0.9243	0.9933	0.9689	0.9623	0.994	Non-Fickian diffusion
F4	0.9151	0.9963	0.9603	0.9503	0.9939	Non-Fickian diffusion

Table 6. *Ex vivo* permeation flux and permeability coefficient of diltiazem buccal patches

Formulation	$t_{50\%}$ (min)	Flux (J_{SS}) (mg/cm ² /hr)	Permeability coefficient (cm/hr)
F1	430	0.666 ± 0.05	0.0666 ± 0.005
F2	401	0.7149 ± 0.027	0.0715 ± 0.003
F3	408	0.6929 ± 0.016	0.0693 ± 0.002
F4	466	0.6269 ± 0.04	0.0623 ± 0.004

$t_{50\%}$: Time required for 50% of diltiazem to be permeated

Drug release from backing layer

Drug release from the backing layer was investigated to ascertain the efficiency of the backing membrane to provide unidirectional release of the drug through the patch. The results of the study showed that no drug was released during the study.

Stability studies

The stability study of F2 was conducted in artificial saliva to mimic the stability of the drug and the formulation in the oral cavity. No color change was observed. Thickness of patches increased to 18.15% owing to swelling in artificial saliva over 6 h (Table 7). The recovery of drug from the patches was 99.5% (9.92 mg) indicating maximum utilization of the drug incorporated.

Accelerated stability studies were performed for optimized formulation (F2) as per ICH Q1A (R2)

cumulative percentage of diltiazem permeated in 12 h was found to be 79.86 ± 3.15%. Flux and permeability coefficient of diltiazem was found to be 0.6913 ± 0.024 mg/cm²/hr and 0.0691 ± 0.002 cm/hr, respectively, for the optimized formulation after stability study.

The *ex vivo* permeation profile of F2 after stability study could be best expressed by zero order model, as the plots showed highest linearity (r^2 : 0.9932) and the obtained release exponent (n) value, 0.9375, supported non Fickian release. From the results, it was observed that there was no change in the best fit model and transport mechanism even after stability study.

Conclusion

A novel mucoadhesive buccal patch of diltiazem hydrochloride with unidirectional drug delivery was developed to overcome the first-pass metabolism and subsequent low bioavailability of the drug. The

Table 7. Stability study of F2 in artificial saliva

Sampling time (hr)	Thickness (μm)	Drug recovered (mg)
0	292 ± 2.64	9.97 ± 0.015
1	307 ± 2.51	9.71 ± 0.02
2	322 ± 3.52	9.85 ± 0.02
3	331 ± 3.06	9.89 ± 0.03
6	345 ± 3.51	9.92 ± 0.02

Mean ± SD, n = 3

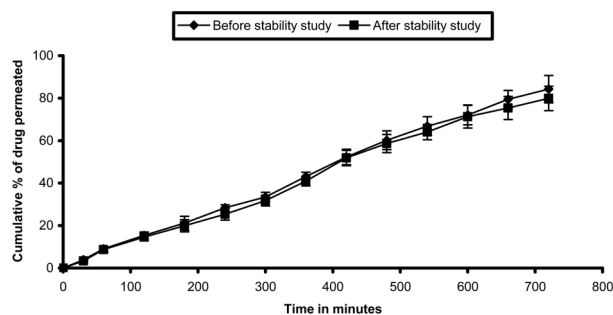
Table 8. Stability study data of F2 patches

Formulation	Drug content (mg)	$t_{50\%}$ (min)	Flux (J_{SS}) (mg/cm ² /hr)	Permeability coefficient (cm/hr)
Before stability	10.21 ± 0.05	401	0.7149 ± 0.027	0.0713 ± 0.003
After stability	9.86 ± 0.57	405	0.6913 ± 0.024	0.0691 ± 0.002

Mean ± SD, n = 3

guidelines at 40 ± 2 °C and 75 ± 5% RH for 6 months. After specified duration, visual examination of the buccal patches did not show any change in morphology. The values of drug content, $t_{50\%}$, flux and permeability coefficient of optimized formulation before and after stability study are depicted in Table 8.

The results of the stability studies revealed that there was a significant change in drug content and *ex vivo* permeation through porcine buccal mucosa. Shelf life of the formulation was calculated by using “Stab R”³⁸⁾ software and it was found to be 22 months. The

Fig. 6. *Ex vivo* drug permeation profile of F2

bioadhesive patch displayed sufficient bioadhesive strength and *in vitro* drug release. The *ex vivo* permeation studies have shown that this is a potential drug delivery system for diltiazem hydrochloride with considerably good stability and release profile. The release of drug was found to be a combination of diffusion and erosion of polymers. So, it is possible to formulate mucoadhesive patches of diltiazem hydrochloride with the intention of obtaining better therapeutic efficiency by sustaining drug release thereby improving patient compliance and increasing bioavailability with decreased dosing.

Conflicts of interest: none.

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